Anti-tumor Effect of Novel Cationic Biomaterials in Prostate Cancer

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Abstract. Background: Tumor cells expressing excessive anionic-charged sialic acid can be potentially targeted by cationic polymers which may inhibit tumor growth. In the present study, three new families of cationic polymers were synthesized to assess their effects on prostate cancer cells. Materials and Methods: Cationic polymers effects on PC3 prostate cancer cells and normal prostate epithelial cell (RWPE-1) were assessed using cell viability, DNA fragmentation, apoptosis assays and confocal microscopy. Results: The dextran-based polymer (Dex-PA-3X) (40 μ g/ml) and the vinyl-based PolyAETA (5 μ g/ml) induced a significant reduction in cell viability in PC3 cells (85% and 50%, respectively; p<0.05) in comparison to RWPE-1 cells. Furthermore, Dex-PA-3X induced a 50%, and PolyAETA induced a 35% increase in cell death in PC3 cells compared to RWPE-1 cells measured by DNA fragmentation assay. Lower concentrations of both polymers induced apoptosis while higher concentrations induced both apoptosis and necrosis by immunostaining. Confocal microscopy indicated the localization of Dex-PA in the cytoplasm of PC3 but not RWPE-1 cells, while PolyAETA was seen in both PC3 and RWPE-1 cells, but at lower intensity in RWPE-1 cells. Conclusion: The newly-synthesized cationic polymers Dex-PA-3X and PolyAETA selectively bind to, reduce viability and induce cell apoptosis in prostate cancer cells, suggesting that targeting negatively-charged tumor cells could be a novel strategy to treat prostate cancer.

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Several studies suggest that malignant cells are more negatively-charged compared with normal cells due to the overexpression of sialic acid on their cell surface (1-4). Tumor cells expressing polysialic acid tend to dissociate from each other due to electrostatic repulsion leading to cell migration into the circulation (5-7), which may contribute to increased invasiveness and metastatic potential (8-10). Sialic acid has a dissociation constant of 2.6, an indication of a strong negative charge at pH 7.4. Consequently, the negatively-charged cell surface attributed to sialic acid on malignant cells may represent a potential drug target. Holmberg et al. reported that the growth of tumor cell lines including prostate cancer cells was inhibited by positivelycharged cationic dextran derivatives (11) in a concentrationdependent fashion, suggesting that positively charged polymers represent a novel strategy to target and inhibit the growth of malignant cells.

A variety of novel positively- and negatively-charged water soluble polymers have recently been synthesized, including polymers derived from natural polysaccharides like chitosan and dextran, from synthetic original like amino acid-based poly(ester amide)s (AA-PEA) and a new class of water soluble cationic polymer (PolyAETA) synthesized from the [2-(acryloxy)ethyl]trimethylammonium chloride] vinyl-based monomer (AETA) (12-25). Many of these polymers have been tested as non-viral gene vectors for transfecting cells (23, 25-27) and scaffolds for supporting cell proliferation (20, 28), while being safely tested in humans for a wide range of biomedical applications ranging from coating for drug-eluting stents (29, 30), synthetic vaccines (31) and drug-eluting fibrous membranes as dressing for treating burn wounds (32).

In the current study, we screened multiple polymers from three families of cationic natural and synthetic polymers (dextran and chitosan from the polysaccharide family, Arg- and Lys-based PEAs from the AA-PEA family and PolyAETA from the vinyl family) for their ability to inhibit growth of prostate cancer cells when compared to the RWPE-1 control.

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Figure 1. Generic chemical structures of the polymers tested. A) Repeating unit structure of a cationic amino acid-based poly (ester amide)s with Arg or Lys as the amino acid building block. B) Multiamino acid-based poly (ester amide)s having both Arg and Lys within the same repeating unit of the AA-PEA polymer. C) Dextran-based cationic polymers and their anionic control. Depending on the R group, Dex-EA, Dex-PA, and Dex-GND are shown. The R -CH₂COOH (Dex-CA) was used as the anionic control for the dextran-based cationic polymers. D) GMA-chitosan-NH₂. Glycidyl methacrylate-chitosan (GMA-chitosan) as the parent polysaccharide and its vinyl end group in the GMA moiety is converted into thioamine to fabricate GMA-chitosan-NH₂. E) Synthetic cationic vinyl polymer, PolyAETA.

Based on the polymer screening data, an in-depth study was performed on two selected candidates to further characterize their biological interactions with prostate cancer cells.

Materials and Methods

Structure of amino-acid based poly (ester) amide polymers, polysaccharide-based polymers and PolyAETA. The structure of the polymers, including chemical formulas are described in the Figure 1 and Table I.

Cell culture and reagents. Both human prostate cancer cell line PC3 and RWPE-1 (normal prostate epithelial cells) were purchased from American Type Culture Collection (Manassas, VA, USA) and maintained as previously described (33). RWPE-1 cells were grown

in Roswell Park Memorial Institute medium (RPMI, Sigma-Aldrich, St. Louis, MO, USA) supplemented with 0.05 mg/ml bovine pituitary extract and 5 ng/ml epidermal growth factor while PC3 cells were kept in RPMI growth medium.

MTT assay. Cell proliferation and viability were measured using CellTiter 96[®] AQ_{ueous} One Solution Cell Proliferation Assay (MTT) (Promega, Madison, Wisconsin, USA) according to the manufacturer's instructions. Briefly, 10⁴ cells in 100 μl RPMI medium were seeded in 96-well plates and cultured in 5% Fetal bovine serum (FBS, Sigma-Aldrich, St. Louis, MO, USA) for 24 hours. The wells were washed once with PBS and 100 μl fresh medium was added with 1% FBS containing each of the polymers shown in the Supplementary Table at 100 μg/ml for 4 days and kept at 37°C, 5% CO₂ incubator. On the day of testing, 15 μl of MTT labelling reagent (5 mg/ml MTT) was added to each well and the mixture was incubated for 2-4 h at 37°C, then 100

 μl of solubilizing reagent was added and the plate was incubated at room temperature (RT) for 2 h or overnight to dissolve formazan crystals. Absorbance was measured at OD_{595} in a Chameleon multilabel detection platform (Hidex Inc., Mustionkatu, Turku, Finland). Each assay was carried out in triplicate and each experiment was repeated at least twice.

DNA fragmentation ELISA assay. PC3 cells were cultured in media containing 5-bromo-2-deoxyuridine (BrdU) reagent (1:1000 from cellular DNA Fragmentation ELISA kit. Roche-applied-science. Tucson, AZ, USA) at 37°C for 2-3 days without changing the medium. Labeled cells were trypsinized and aliquoted into a 96-well microplate at a concentration of 1×10⁵ cells/ml in RPMI medium with 10% FBS, and washed once with PBS on the second day before adding 100 µl fresh RPMI medium supplemented with 1% FBS. Dex-PA-3X (10, 40 and 160 µg/ml) and PolyAETA (2.5, 5 and 10 µg/ml) were individually added into the RPMI medium for 24 h, the microplate centrifuged for 5 min and the supernatants added to a fresh testing microplate previously coated with anti-DNA antibody. The plate was placed on a shaker at 200 rpm for 90 min at RT, washed with washing buffer 3 times, microwaved for 4 min, cooled down at RT, placed at -20°C for 10 min and then washed with washing buffer. Anti-BrdUperoxidase was then added and incubated at RT for 90 min on a rotator. The plate was washed 3 times and 100 µl substrate solution added and absorbance was measured at wavelength 370 nm with the reference wavelength of 492 nm. Each assay was carried out in triplicate and each experiment was repeated at least twice.

Propidium iodide (PI) staining. To detect necrosis induced by polymers, PC3 cells were seeded on the coverslips in a 12-well plate (Thermo Fisher Scientific, Waltham, MA, USA), and cultured in RPMI medium with 10% FBS overnight, washed with PBS and incubated in media containing PolyAETA at 5 and 20 μg/ml or Dex-PA-3X at 40 and 160 μg/ml for 24 h. Following incubation, cells were washed with PBS, stained with 10 μg/ml Propidium iodide (PI; Invitrogen, Grand Island, NY, USA) for10 min at RT, washed with PBS and fixed with 4% paraformaldehyde for 20 min at RT. After fixation, cells were rinsed twice with distilled water and stained with 0.5 μg/ml DAPI (4', 6-Diamidino-2-Phenylindole, Dilactate, Sigma-Aldrich, St. Louis, MO, USA) for 2 min. After washing with distilled water, slides were dried and mounted for fluorescence microscopy. PInegative were considered live and apoptotic cells and PI-positive were considered necrotic and "apoptonecrotic" cells.

Cleaved caspase-3 immunofluorescence staining. PC3 cells were seeded on coverslips in a 12-well plate and incubated with media containing Dex-PA-3X (40 and 160 μg/ml) and PolyAETA (5 and 20 μg/ml) for 24 h and cells were fixed with 4% formaldehyde for 15 min at RT, rinsed three times in PBS for 5 min each, incubated in blocking buffer (4% BSA in PBS) for 60 min, washed and then incubated in cleaved caspase-3 (Asp175) antibody (Alexa Fluor® 488 Conjugate; Cell Signaling Technology, Danvers, MA, USA) diluted 1:100 in the dilution buffer for 60 min at RT. Cells were rinsed three times in PBS for 5 min and the coverslips were mounted with Prolong® Gold Antifade Reagent (Thermo Fisher Scientific, Waltham, MA, USA) and observed under fluorescence microscopy immediately.

Immunofluorescence and confocal microscopy. To determine cellular localization of polymers, PolyAETA and Dex-PA-1X were fluorescently conjugated. Due to the consumption of all the available

Table I. List of polymers.

AA-PEA family (Net charge)	Polysaccharide family (Net charge)	Vinyl-based family (Net charge)
2A3S	Dex-EA	*PolyAETA
4A3S	*Dex-PA1x	PAA
4A3ES	Dex-PA3x	
8A7ES	Dex-GND	
2A4L-25	GMA-NH2	
4L4NH2	Dex-CA	

All the polymers are positively charged except Dex-CA and PAA (negatively charged) used as controls. *Polymers used for in-depth analysis.

hydroxyl groups in the Dex-PA-3X, no free hydroxyl groups could be used to conjugate a fluorescence dye onto Dex-PA-3X. PC3 and RWPE-1 cells grown on coverslips in 48-well plates in RPMI media were incubated with 100 µg/ml fluorescently conjugated PolyAETA and Dex-PA-1X for 30 min, and 5 h, rinsed with PBS and fixed with 2% paraformaldehyde for 20 min. After washing with PBS, cells were blocked with 2.5% BSA in PBS for 1 h and then incubated with Alexa fluor 568 labeled mouse anti-EpCAM (BioLegend, San Diego, CA, USA) 1:100 overnight at 4°C. Cells were washed with PBS, incubated in DAPI for 5 min, rinsed with distilled water and analyzed by a confocal microscope (Carl Zeiss LSM 510 META, Narashige, MN, USA) for localization of the polymers inside the cells.

Statistical analysis. The level of significance was considered at p<0.05 using Student's t-test analysis. All data are presented as mean \pm S.D. of at least three independent experiments from different batches of cultures. Figures are representative of one triplicate experiment.

Results

Effect of polymers on cell viability in prostate cells. For a rapid in vitro polymer screening of prostate cancer cells, PC3 cells were incubated with a fixed concentration (100 μ g/ml) of different cationic and anionic polymers and cell viability was measured at 4 days using an MTT assay (Figure 2). Among the 12 cationic polymers tested, PolyAETA (vinylbased) and Dex-PA (polysaccharide-based) showed a significant reduction in cell viability, with only <20% PC3 cells viable (p<0.05). AA-PEA polymers had little or no effect compared to the PBS control. Figure 1 provides the chemical structure of all tested polymers.

Dex-PA-3X and PolyAETA polymers were further analyzed at various concentrations on RWPE-1 normal prostate epithelial cells and PC3 cells. Dex-PA-3X showed an 85% and 88% decrease (p<0.05) in the cell viability in PC3 cells in comparison to RWPE-1 cells at 40 and 160 µg/ml, respectively (Figure 3A). Similarly, PolyAETA showed a significant decrease (45%, p<0.05) in cell viability in PC3 cells in comparison to RWPE-1 cells at 5 µg/ml (Figure 3B)

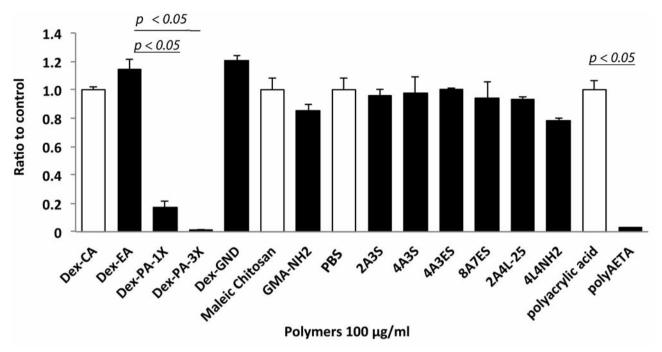


Figure 2. MTT assay was performed to screen the effect of different polymers on PC3 cells. Refer to Table I for the testing polymers. Vertical axis indicates the ratio of viable cells of testing polymers to their corresponding controls that were set at the value 1. Therefore, the lower the bars, the more effective are the polymers in reducing cancer cell viability. PBS was used as the control for all AA-PEA-based cationic polymers since no water soluble anionic AA-PEAs could be synthesized. The plain white bars are controls for the respective polymers which are black bars next to them. After incubated with PC3 cells for 96 hours at the indicated concentration, Dex-PA-1X, Dex-PA-3X and PolyAETA showed a prominent effect in reducing viability of PC3 cells comparing to the other polymers. Both Dex-PA-1X and 3X belong to polysaccharide, while PolyAETA belongs to vinyl-based family.

while at 20 μ g/ml, both RWPE-1 and PC3 cells showed a similar reduction in cell viability. These data showed that both polymers inhibit PC-3 cells more than RWPE-1 cells.

Characterization of polymer-induced cell death in prostate cells. We next examined the effects of PolyAETA and Dex-PA-3X on inducing apoptosis. PC3 and RWPE-1 cells were treated with Dex-PA-3X for 24 h at 40 and 160 µg/ml concentrations (Figure 4A). Dex-PA-3X induced a 50% increase in apoptosis in PC3 cells compared with RWPE-1 cells at both 40 and 160 μ g/ml (p<0.05), as determined by DNA fragmentation ELISA assay. PolyAETA at 5 and 20 μg/ml induced a 35% increase in apoptosis in PC3 cells in comparison with RWPE-1 cells (Figure 4B, p<0.05). To further explore the mechanism of PolyAETA and Dex-PA-3X induced cell death, PI and caspase-3 staining was performed on PC3 cells. As shown in Figure 5, cationic Dex-PA-3X at 40 µg/ml induced cell death in PC3 cells mainly by apoptosis while at 160 µg/ml cell death was induced both by necrosis and apoptosis (Figure 5A). Similarly, PolyAETA at 5 µg/ml induced cell death primarily by apoptosis, while at 20 μg/ml, both necrosis and apoptosis were observed. In comparison to Dex-PA-3X (160 μg/ml), PolyAETA (20 μg/ml) induced more necrosis in PC3 cells.

Localization of the polymers in RWPE-1 and PC3 cells. Confocal microscopy was performed to determine where polymers were localized in cells following binding to the cell surface. At 1 h, both Dex-PA-1X and PolyAETA were localized in the cytoplasm of PC3 cells and to a much lesser extent in RWPE-1 cells (Figure 6), supporting the hypothesis that the presence of negatively charged cell surface sialic acid on cancer cells permits a more robust interaction and internalization of cationic polymers in comparison to non-malignant cells. After 5 h, the amount of both PolyAETA and Dex-PA-1X polymers increased in the cytoplasm of PC3, but not RWPE-1 cells (Figure 6A and 6B).

Discussion

In the present study, a number of new cationic and water soluble polymers ranging from natural-based like dextran and chitosan to synthetic like poly(AETA) and AA-PEAs were synthesized to examine their effect on prostate cells. The cationic polymers were synthesized based on the hypothesis that tumor cells express higher amounts of sialic acid than normal cells generating a higher negative charge on their cell surfaces that would facilitate uptake of cationic compounds.

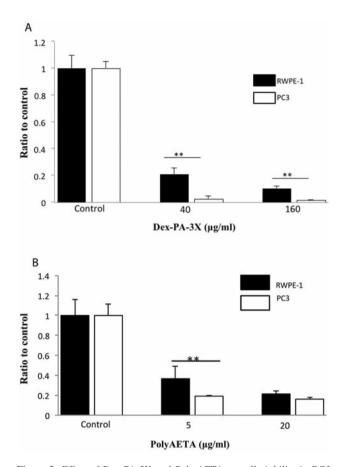


Figure 3. Effect of Dex-PA-3X and Poly AETA on cell viability in PC3 and RWPE-1 cells. A) PC3 and RWPE-1 cells were treated with Dex-PA-3X for 24 h at indicated concentrations with Dex-CA as control. As shown, Dex-PA-3X is far more cytotoxic to cancerous PC3 cells than to normal prostate epithelial RWPE-1 cells at both concentrations of 40 and 160 µg/ml. A 85% and 88% more reduction in cell viability were induced in PC3 cells than in RWPE-1 cells by Dex-PA-3X at 40 µg/ml and 160 µg/ml, respectively. **p<0.05. B) PC3 and RWPE-1 cells were treated with PolyAETA for 24 h at indicated concentrations with polyacrylic acid as control. As shown, PolyAETA is significantly more cytotoxic to cancerous PC3 cells than to normal prostate epithelial RWPE-1 cells at the concentrations of 5µg/ml. About 45% more reduction in cell viability was induced in PC3 cells than in RWPE-1 cells by PolyAETA at 5 µg/ml. **p<0.05.

Sialic acids are a group of neuraminic acid widely present as sugars on the terminal positions of glycoproteins or glycolipids. Overexpression of sialylated antigens has been commonly observed in several epithelial cancers such as gastric, pancreatic, breast, ovarian and colorectal, and usually linked with poor prognosis (34). The poor prognosis may be due to increased metastatic potential of tumors expressing sialic acid as sialyl-glycoconjugates regulate adhesion and promote motility, while inhibition of sialylation reduces the metastatic potential of cancer cells (35).

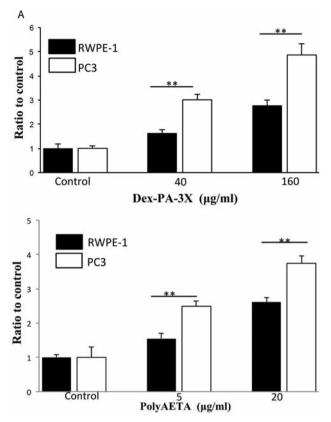


Figure 4. Effect of Dex-PA-3X and PolyAETA on cell apoptosis in PC3 and RWPE-1 cells. A) PC3 and RWPE-1 cells were treated with Dex-PA-3X for 24 h at 40 and 160 µg/ml concentrations. A significant increase in cell death was seen in PC3 cells compared to RWPE-1 cells at all concentrations. **p<0.05. B) PC3 and RWPE-1 cells were treated with PolyAETA for 24 h at 5 and 20 µg/ml concentrations. A significant increase in cell death was seen in PC3 cells compared to RWPE-1 cells at all concentrations. **p<0.05. PC3 and RWPE-1 cells were treated with Dex-PA-3X for 24 h at 40 and 160 µg/ml concentrations. A significant increase in cell death was seen in PC3 cells compared to RWPE-1 cells at all concentrations. **p<0.05.

Among the 12 cationic polymers examined in the current study, Lys-PEAs, GMA-chitosan-NH₂, maleic chitosan (as the control to GMA-chitosan-NH₂), Dex-GND and Poly (AETA) are being reported for the first time, and the remaining were synthesized according to prior published studies (13, 14, 19, 23, 26, 27). In the present study, we tested the effect of cationic polymers in both cancerous and non-cancerous prostate cells, while prior published studies did not test the relative efficacy of cationic polymers in malignant versus non-malignant prostate cells (11, 36-38).

Based on our results, the cytotoxicity of cationic polymers can be ranked as follows; Dex-PA-3X> PolyAETA> Dex-PA-1X> 4L4NH2> GMA-NH2> 2A4L-25> 8A7ES> 2A3S> 4A3S> 4A3ES> Dex-EA> Dex-GND. Dex-PA-3X and

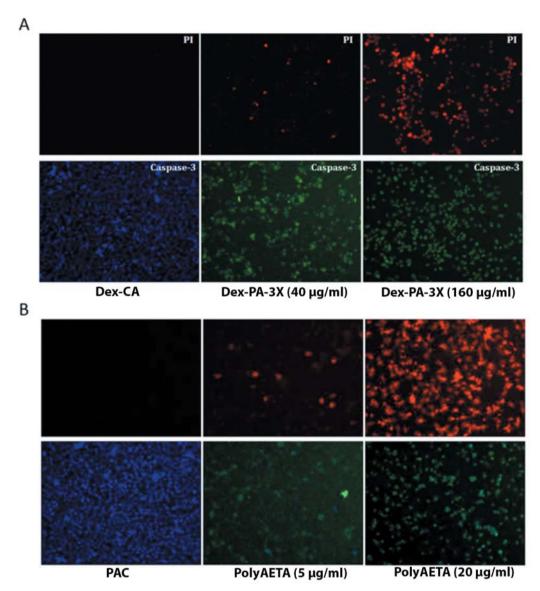


Figure 5. Propidium iodide and cleaved caspase-3 staining for cell death induced by PolyAETA and Dex-PA-3X. Cells undergoing necrosis or necroptosis are stained red with propidium iodide (PI) and cells undergoing apoptosis are stained green with cleaved caspase-3 antibody. DAPI was used to stain the nuclei of all cells: A) PC3 cells treated with Dex-PA-3X for 24 h at indicated concentrations. B) PC3 cells treated with PolyAETA for 24 h at indicated concentrations. PAA and Dex-CA were used as controls for PolyAETA and Dex-PA-3X respectively.

PolyAETA belonging to dextran-based and vinyl-based class of polymers, respectively, demonstrated the most significant cytotoxic effects.

Among polysaccharides, Dex-PA showed an increased cytotoxicity than Dex-EA which could be due to the: (i) presence of increased number of free amino end groups; (ii) longer spacer between the free amino end group and the dextran backbone; or (iii) hydrophobic nature of propylamine-pendant group allowing for better interaction with the cell membrane. The lack of cytotoxicity of the cationic Dex-GND

toward PC3 cells can be attributed to the presence of the pendant guanidine group as found in Arg-PEAs. The difference in PC3 cell cytotoxicity between Dex-PA-1X and Dex-PA-3X could result from an increase in the propylamine concentration. In Dex-PA-3X, all the 3 -OH groups in the dextran repeating unit were substituted by propylamine, while only one out of three -OH groups in the Dex-PA-1X repeating unit was substituted by propylamine. Similarly it was shown that a cationic dextran derivative with 25% amine substitution resulted in more cell death than 22% amine substitution at

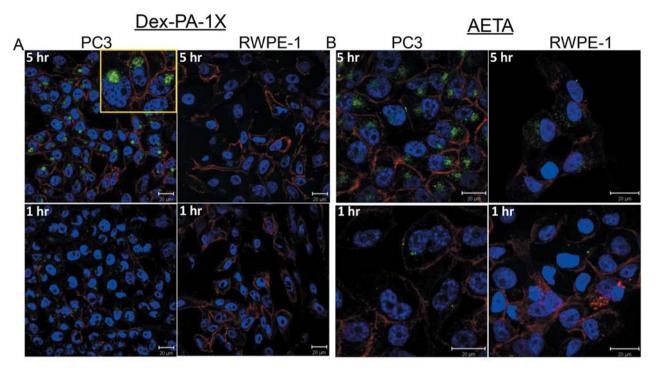


Figure 6. Confocal microscopy showing the localization of Dex-PA-1X and PolyAETA in PC3 and RWPE-1 prostate cells. Both PolyAETA and Dex-PA-1X was used at 100 µg/ml. A) Localization of Dex-PA-1X at 1 and 5 h. Dex-PA-1X starts appearing in the cytoplasm of PC3 cells at 1 h and its concentration inside the cytoplasm increases with time. On the contrary, no Dex-PA-1X is seen in RWPE-1 cells at any time point used in the study. Red= EpCAM, Green= Dex-PA-1X. B) Localization of PolyAETA in PC3 and RWPE-1 cells at similar time points as in A. PolyAETA is concentrated more in PC3 cells at 5 h in comparison to RWPE-1 cells. Red= EpCAM, Green= PolyAETA.

similar concentrations (11). Azab *et al.* also reported that the percentage binding of the cationic polymer was increased when the charge density of the cationic polymers was increased by substituting more cations and that this binding was reduced in the presence of neuraminidase (removes sialic acid) (36).

The cationic property of PolyAETA, a vinyl-based nonbiodegradable synthetic cationic polymer, comes from the pendant quaternary ammonium salt which retains its cationic charge over most of the pH range. Raffaghello et al. reported that polyvinyl alcohol-based polymers also showed a potent cytotoxicity toward neuroblastoma and melanoma cell lines via the induction of caspase signaling followed by apoptosis (39). In contrast, AA-PEA polymers did not demonstrate cytotoxicity, which may result from the cationic nature of the pendant guanidine group of arginine, having a pKa of 12.5. This lack of adverse effect from the guanidine group is consistent with our screening data in which the -OH groups of the dextran, was substituted by the pendant guanidine group Dex-GND, which showed higher PC3 cell proliferation than the control. Meurling et al. also reported that free (unconjugated) guanidine compound showed no adverse effect on the tumor cell growth of bladder cancer cell lines even at mM concentrations (38).

The mechanism of cytotoxicity caused by cationic polymers is not fully-understood. Because of their growth inhibitory effects on PC-3 cells, we further evaluated cells treated with Dex-PA and PolyAETA. At lower concentrations of polymer, cell death was induced *via* activation of caspase signaling, whereas at higher concentrations, a significant amount of necrosis was observed. Several studies have shown that dextran-based polymers or drugs coupled to these polymers can be used to induce apoptosis or to inhibit proliferation of malignant cells (40-45). Marquez *et al.* showed a 100% cell death in PC3 cells using a cationic dextran as detected by fluorimetric cytotoxicity assay (11).

The increased cytotoxic and apoptotic effect of the polymers on PC3 cells in comparison with RWPE-1 cells may be due to the differential expression of sialic acid on their respective cell surfaces. Marquez *et al.* (2004) indirectly showed the presence of sialic acid on PC3 cells as determined by binding of the FITC-labeled lectin. However, no control cell line, such as normal prostate cells were used in that study (11). In the present study, confocal laser scanning microscopy data revealed the presence of both PolyAETA and Dex-PA-3X in the cytoplasm of PC3 cells to a larger extent than RWPE-1 cells. This also supports our data showing higher

cytotoxicity and apoptosis in PC3 cells in comparison to RWPE-1 cells. Our localization study, however, cannot validate Marquez *et al.*' findings that the cytotoxicity of these cationic polymers was due to their preferential binding onto cancer cell membranes that could disrupt cell proliferation, since we did not observe apparent cell membrane localization of the cationic polymers (11). Another study conducted by Azab *et al.* showed that SW620, a highly metastatic colon cancer cell line, demonstrated more binding of the cationic polymer than SW480, a less aggressive colon cancer cell line (36). Furthermore, in the presence of neuraminidase, the percentage of bound cationic polymer was markedly reduced in SW620 cells compared with SW480 cells.

Overall, the data suggest that cationic and water-soluble polymers may have the potential to differentially target malignant prostate cells *versus* non-malignant cells based on the differences in their cell surface charges. Further exploration of the use of these polymers as a drug-alone or as a vector for therapeutic drug delivery is required.

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